

The benefits evaluation of abdominal deep inspiration breath hold based on knowledge-based radiotherapy treatment planning for left-sided breast cancer

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Research

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23 **Abstract**

24 **Purpose:** Study the impact of abdominal deep inspiration breath hold (DIBH)
25 technique on knowledge-based radiotherapy treatment planning for left-sided breast
26 cancer to guide the application of DIBH radiotherapy technology.

27 **Methods and Materials:** Two kernel density estimation (KDE) models were
28 developed based on 40 left-sided breast cancer patients with two CT acquisitions of
29 free breathing (FB-CT) and DIBH (DIBH-CT). Each KDE model was used to predict
30 DVHs based on DIBH-CT and FB-CT for another 10 new patients similar to our
31 training datasets. The predicted DVHs were taken as a substitute to dose constraints
32 and objective functions in the Eclipse treatment planning system, with the same
33 requirements for the planning target volume (PTV). The mean doses to the heart, the
34 left anterior descending coronary artery (LADCA) and the ipsilateral lung were
35 evaluated and compared using the T-test among clinical plans, KDE predictions, and
36 KDE plans.

37 **Results:** Our study demonstrated that the KDE model can generate deliverable
38 simulations equivalent to clinically applicable plans. The T-test was applied to test the
39 consistency hypothesis on another 10 left-sided breast cancer patients. In cases of the
40 same breathing status, there was no statistically significant difference between the
41 predicted and the clinical plans for all clinically relevant dose volume histogram
42 (DVH) indices ($p > 0.05$), and all predicted DVHs can be transferred into deliverable
43 plans. For DIBH-CT images, significant differences were observed in D_{mean} between
44 FB model predictions and the clinical plans ($p < 0.05$). DIBH model prediction cannot

45 be optimized to a deliverable plan based on FB-CT, with a counsel of perfection.

46 **Conclusion:** This study demonstrated that the KDE prediction results were well fitted
47 for the same breathing condition but degrade with different breathing conditions. The
48 benefits of DIBH can be evaluated quickly and effectively by the specific
49 knowledge-based treatment planning for left-sided breast cancer radiotherapy. This
50 study will help to further realize the goal of automatic treatment planning.

51 **Keywords:** Deep inspiration breath hold, dose distribution prediction,
52 knowledge-based planning, machine learning, breast cancer

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57 **Background**

58 Postoperative adjuvant radiotherapy (RT) plays an indispensable role in
59 breast-conserving treatment to minimize the risks of local-regional recurrence and
60 metastasis. Whole breast irradiation (WBI) after breast-conserving surgery as a
61 comprehensive treatment model, which has been confirmed to possess the similar
62 local control and overall survival rates to modified radical surgery in breast cancer
63 patients^[1]. However, the dose of the surrounding critical organs-at-risks (OARs),
64 especially the heart, left lung and the left anterior descending coronary artery
65 (LADCA)^[2-4], are crucial to the RT quality assessment for left-sided breast cancer.

66 Therefore, by using diversity of methods, such as DIBH, intensity-modulated

67 radiation therapy (IMRT) techniques, treatment in the prone position and proton
68 therapy, to shield the heart and minimize the lung and LADCA doses while ensuring
69 enough dose in the target volume during left breast postoperative radiotherapy have
70 been presented. Combining DIBH and IMRT is the most commonly-used strategy in
71 left-sided breast postoperative radiotherapy^[5-7]. The DIBH maneuver we used is the
72 abdominal DIBH (A-DIBH), which could widen the spatial Euclidean distances
73 between the heart and the target volume. IMRT treatment technique has the capability
74 of reducing the cardiac dose while delivering adequate target coverage because of its
75 unique dose calculation and beam weight optimization.

76 The selection of the final radiotherapy regimen (especially the selection of
77 respiratory mode) will greatly affect the normal tissue complications (NTCP) and
78 tumor control rate^[8,9]. In the past IMRT plans, physicians often determined the ideal
79 OARs dose-volume limit through population-based recommendations (either from the
80 tumor radiotherapy team or from the doctor's intuition)^[10]. However, the huge
81 geometric differences in the complexity of PTV and OAR among patients make it a
82 challenge for doctors to quickly and accurately select the best ultimate treatment for a
83 particular patient within all acceptable options.

84 Knowledge-based planning (KBP) is a promising technology. There is a large
85 amount of image information and dose planning information of cancer patients in the
86 current radiotherapy system, which has become a priori knowledge. By feature
87 extraction and quantitative analysis of these prior knowledge, a reliable empirical
88 model (KBMs) can be obtained to realize the intelligence of the radiotherapy planning

89 system. Current studies have proved that KBP has a higher consistency of plan quality
90 and higher operational efficiency than manual plans with different quality ^[11-13]. For
91 example, RapidPlan™(Varian Medical Systems, Palo Alto, CA, USA) has been
92 widely used as a commercial KBP product ^[11,14].

93 In the KBP method, the prediction of DVH in new patients requires the use of
94 the DVH of OAR in the previous clinical plan and the parameterized model generated
95 by the relevant anatomical structure ^[13,17], thus emphasizing the importance of the
96 parameterized prior model. However, it remains to be seen whether the
97 implementation effect of the parameterized prior model in KBP is consistent under
98 different breathing conditions. To our best knowledge, the impacts of different
99 breathing methods during CT simulation for left-sided breast cancer on
100 knowledge-based treatment planning have not been reported before.

101 Therefore, this study established two knowledge-based empirical models for the
102 treatment of the same group of breast cancer patients based on different respiratory
103 conditions. We then used these two KBMs to cross-predict CT in both breathing
104 patterns, creating four KBP plans for each patient. We attempted to investigate the
105 compatibility of KBP with different respiratory conditions, such as whether the DIBH
106 KBM is applicable to FB-CT prediction, or whether the FB KBM is applicable to
107 DIBH-CT prediction. Quantifying the benefits of using the specified model can help
108 us clearly understand the use of KBM to predict the OAR dose of postoperative
109 radiotherapy for breast cancer and guide the application of A-DIBH radiotherapy
110 technology.

111 **Methods**

112 The workflow of this study is illustrated in the diagram on Figure 1. Firstly, two
113 KBMs (FB model and DIBH model) were built from 40 existing clinical plans that
114 have ideal tumor coverage and OAR doses with different breath settings. Another 10
115 new patients were selected to investigate the performance of the prediction model.
116 Two treatment plans were established with uniform standards by the experienced
117 physicist, and then confirmed by another senior physicist.

118 DVHs of these 10 new patients were estimated by two KBMs. The estimated
119 DVHs were taken as a substitute to dose constraints and objective functions in Eclipse
120 treatment planning system (TPS) for each new patient.

121 There are three types of comparisons we want to investigate in this study. Firstly,
122 we want to confirm whether our model can precisely predict the DVHs with same
123 breath settings, such as using FB model to predict patients with FB CT. These
124 comparisons were marked as 'green' in Figure 1.

125 Secondly, we want to investigate whether model build with one breath condition
126 can precisely predict DVH for patients with another breath. Such as using FB model
127 to predict the DVH for the patient with DIBH CT images. These comparisons were
128 marked as 'blue' in Figure 1.

129 Third, we want to investigate whether these DVH prediction models can be
130 optimized to a deliverable plan. These comparisons were marked as 'red' in Figure1.

131

THE WORKFLOW OF THIS STUDY		PERFORMANCE EVALUATION	
<div style="text-align: center;"> Two CT scans (FB and DIBH) ↓ Model training (FB and DIBH) ↓ Model cross prediction ↓ Performance evaluation </div>	FB-CT	FB model	DIBH model
		Clinical plan VS. KDE prediction	Clinical plan VS. KDE prediction
	DIBH-CT	KDE plan VS. KDE prediction	KDE plan VS. KDE prediction
		Clinical plan VS. KDE prediction	Clinical plan VS. KDE prediction
		KDE plan VS. KDE prediction	KDE plan VS. KDE prediction

Figure 1: The strategy of knowledge-based planning generated optimization objectives

I. Patients and treatment planning

The training dataset consisted of 40 consecutive previously administered by adjuvant RT following breast-conserving surgery for the left-side breast carcinoma. The mean age of those patients was 45.7 (range, 28–70), and the median age was 49. Each patient underwent two CT simulation scans with a Siemens Sensation Open 24-slice scanner (Siemens, Forchheim, Germany): the FB condition and the A-DIBH condition. For consistency, all patients were practiced A-DIBH according to audio and visual coaching for at least a week before the simulation scan, until they can repeat the mode and hold their breath for 15-20s with the auxiliary of Varian Real-time Position Management (RPM) System.

To achieve optimal homogeneity of the data in the present analysis, we incorporated only the whole-breast irradiation series. Target volumes and OAR were entirely contoured via two CT series in the Eclipse treatment planning system (Varian Medical Systems, Palo Alto, CA, USA) according to the Danish Breast Cancer Cooperative Group (DBCG) atlas^[18]. Two intensity modulated radiotherapy treatment plans were generated in the Eclipse for each CT, using the anisotropic analytical

151 algorithm (AAA) for final dose calculation. All IMRT plans containing 6 fixed
152 non-opposing fields with the same gantry angles and beam energies as the clinical
153 methods.

154 The criterion of treatment plans was that 97% of the PTV should be covered by
155 at least 95% of the isodose (and < 108% of the isodose), and the mean dose of PTV in
156 the whole cases was prescribed to 50 Gy in 25 fractions.

157 **II. KDE Model training**

158 Inspired by Skarpman's KDE algorithm^[17], two KDE prediction models were
159 developed based on 40 left-sided breast cancer patients with two different CT scans of
160 FB and DIBH in the aforementioned high-quality IMRT cases. These cases were
161 planned by the experienced dosimetric and approved for clinical treatment by
162 attending physicians. Each KBM was applied to its training dataset then. The
163 estimated DVH was compared with the clinical DVH to verify the reliability of the
164 KDE model.

165 **III. DVH prediction and plan optimization**

166 Another 10 patients similar to our training datasets were enrolled for different
167 model evaluation. Each patient has two images, FB-CT and DIBH-CT. The DVHs of
168 each image was estimated by two KDE models, FB and DIBH model. So, each patient
169 has four estimated DVHs, marked as KDE predictions.

170 To demonstrate whether these estimated DVHs can be directly used to generate
171 deliverable plans, we created another four plans based on four cross-estimated DVHs.
172 We use the estimated DVHs generated in the previous step as dose constraints and

173 objective functions at the specific points without any additional auxiliary human
 174 intervention (Table 1). The KDE plan was optimized on the Eclipse treatment
 175 planning system then. The gantry angles of these plans were exactly the same as the
 176 original clinical plans.

177

178 **Table 1:** OAR dose constraints points used for plan optimization for 200 Gy/fx plan
 179 in 25 fractions.

Organ	Dose constraints points					
Heart	D2%	D _{mean}	V5	V10	V20	V30
LAD	D2%	D _{mean}	V5	V10	V20	V30
Lung	D2%	D _{mean}	V5	V10	V20	V30
Spinal Cord			D _{max}	D _{mean}		
PTV			D _{max}	D _{mean}	D _{min}	

180

181 Each new patient has four KDE predictions, four KDE plans, and two clinical plans.
 182 Here we use superscript to identify plan type and use a subscript to identify the
 183 image. For example, the original clinical plans were marked as $Plan_{FB-CT}^{manual}$ and
 184 $Plan_{DIBH-CT}^{manual}$, KDE plans based on FB-CT were marked as $Plan_{FB-CT}^{FB\ mod\ el}$ and
 185 $Plan_{FB-CT}^{DIBH\ mod\ el}$ for two KBMs, plans based on DIBH-CT were marked as $Plan_{DIBH-CT}^{FB\ mod\ el}$
 186 and $Plan_{DIBH-CT}^{DIBH\ mod\ el}$ for two KBMs. It is noticeable that in all IMRT plans, the PTV
 187 requirements were the same.

188

189 **IV. Dosimetric comparison**

190 A paired student's T-test was used to assess the significance of any differences in
 191 dose metrics where significance corresponded to a p-value 0.05. Mean doses to the
 192 heart, left anterior descending coronary artery (LADCA), and left lung were
 193 compared.

194

195 **Results**

196 **I. The performance of the KDE models**

197 The results (Table2) show that there were no differences between clinical plans
198 and KDE predictions for both models in the training dataset, confirming that the DVH
199 estimation of the KBM was successful.

200

201 **Table 2:** Summary of OAR doses from IMRT validation, comparing the clinical plan
202 and DVH estimates from its KBM for 40 cases (mean \pm SD).

Structure (Average dose)	CT	Clinical plan (Gy)	KDE prediction (Gy)	Clinical plan vs. KDE prediction (p-value)
Heart	FB	1.96 \pm 0.26	1.95 \pm 0.34	0.77
	DIBH	1.30 \pm 0.31	1.31 \pm 0.23	0.87
LADCA	FB	16.57 \pm 0.33	16.02 \pm 0.28	0.48
	DIBH	8.59 \pm 3.73	8.47 \pm 3.08	0.76
Left lung	FB	5.53 \pm 1.42	5.48 \pm 1.15	0.48
	DIBH	5.43 \pm 0.59	5.48 \pm 0.60	0.78

203 *Note: Clinical plan represents the plan used in the model training dataset.*

204

205 **II. The models work in same breath settings**

206 The results of model performance in the same breath settings for another 10
207 left-breast patients were presented in Table 3. There was no difference between
208 clinical plan and estimated plan for all structures' mean dose ($p > 0.05$). Meanwhile,
209 all estimated DVHs can be transferred into deliverable KDE plans. No difference
210 between prediction and KDE plan was observed ($p > 0.05$).

211

212

213 **Table 3:** The comparison of the OAR average doses among the clinical plans,
 214 generated plans and the predicted DVHs performed on the same breath settings (mean
 215 \pm SD) (Gy).

Structure	CT	Clinical plan (Gy)	KDE prediction (Gy)	KDE plan (Gy)	Clinical plan vs. prediction (p-value)	prediction vs. KDE plan (p-value)
Heart	FB	2.03 \pm 0.38	2.00 \pm 0.37	2.04 \pm 0.38	0.94	0.41
	DIBH	1.17 \pm 0.31	1.27 \pm 0.21	1.29 \pm 0.21	0.14	0.29
LADCA	FB	17.46 \pm 5.01	16.01 \pm 1.08	16.00 \pm 1.20	0.35	0.16
	DIBH	6.70 \pm 4.78	7.66 \pm 1.60	7.79 \pm 1.70	0.37	0.06
Left lung	FB	4.73 \pm 1.62	5.41 \pm 0.90	5.44 \pm 0.99	0.11	0.35
	DIBH	4.88 \pm 1.05	5.48 \pm 0.59	5.46 \pm 0.64	0.14	0.23

216

217 III. The FB model works with DIBH-CT

218 The result of the FB model works with DIBH-CT was presented in Table 4. The
 219 mean dose of which the FB model predicted was higher than the clinical plan ($p <$
 220 0.05 for all three structures). By transferring to deliverable KDE plan, the mean dose
 221 of the left lung was reduced significantly ($p = 0.01$).

222

223 **Table 4:** The results of the FB model performed on DIBH-CT in 10 new left-breast
 224 IMRT plans (mean \pm SD) (Gy).

Structure	Clinical plan (Gy)	KDE prediction (Gy)	KDE plan (Gy)	Clinical plan vs. KDE prediction (p-value)	KDE prediction vs. KDE plan (p-value)
Heart	1.17 \pm 0.31	1.42 \pm 0.26	1.40 \pm 0.26	0.01	0.07
LADCA	6.70 \pm 4.78	12.1 \pm 1.61	11.98 \pm 1.51	0.003	0.09
Left lung	4.88 \pm 1.05	5.61 \pm 1.08	5.24 \pm 0.58	0.0002	0.01

225

226 IV. The DIBH model works with FB-CT

227 Table 5 shows the result of the DIBH model works with FB-CT. Compared to
 228 the clinical manual plans, the KDE prediction resulted in lower mean doses of the
 229 heart and LADCA by 0.24 ± 0.36 Gy ($p = 0.02$), and 4.57 ± 2.46 Gy ($p = 0.014$),
 230 respectively. The left lung mean dose of the KDE prediction was 0.33 ± 0.99 Gy
 231 higher than the clinical plan ($p = 0.01$).

232 Significant differences were observed in all structures between the KDE plan and
 233 KDE prediction ($p < 0.05$ for all three structures). These predicted DVHs may not be
 234 directly transferred to a deliverable plan.

235

236 **Table 5:** The results of the DIBH model performed on FB-CT in 10 new left-breast
 237 IMRT plans (mean \pm SD) (Gy)

Structure	Clinical plan (Gy)	KDE prediction (Gy)	KDE plan (Gy)	Clinical plan vs. KDE prediction (p-value)	KDE prediction vs. KDE plan (p-value)
Heart	2.03 ± 0.38	1.79 ± 0.31	2.09 ± 0.35	0.02	0.04
LADCA	17.46 ± 5.01	12.89 ± 1.85	17.86 ± 4.09	0.014	0.002
Left lung	4.73 ± 1.62	5.06 ± 1.01	5.69 ± 1.50	0.01	0.04

238

239 Discussion

240 Deep-inspiration breath-hold offers increased lung volume and suppressed
 241 respiratory motion. As Schönecker et al.^[19] mentioned, DIBH could significantly
 242 reduce high dose areas and mean doses to the heart. Our study also proves the earlier
 243 results, the great significance of abdominal deep inspiration breath hold in protecting
 244 OARs was shown, during radiation for left-sided breast cancer treatment. However,
 245 DIBH treatments may introduce more setup uncertainties such as unsuccessful

246 guidance, resulting in more resource-intensive than FB treatments.

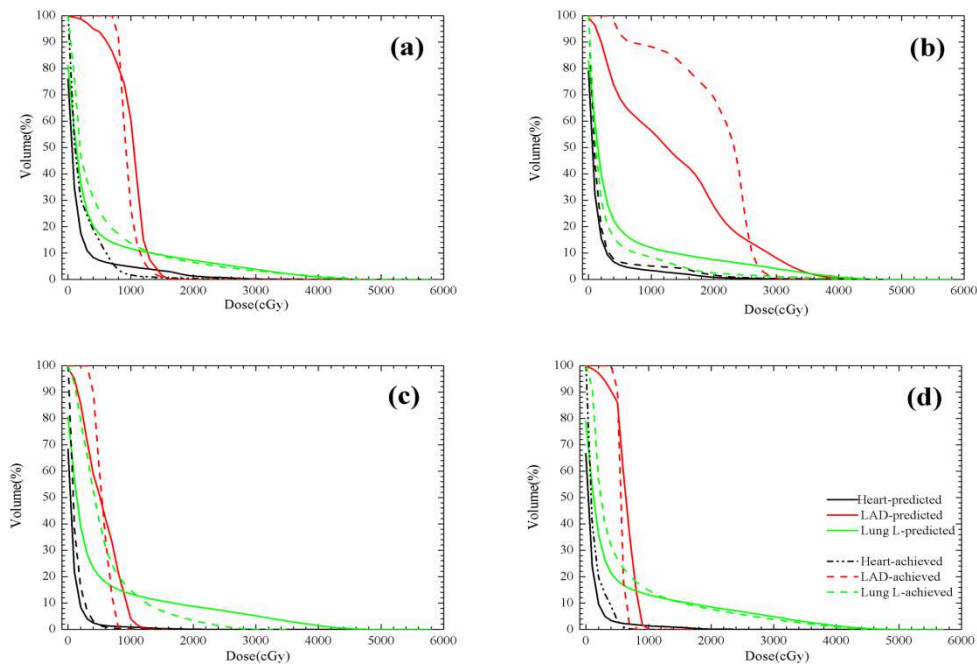
247 It is important to determine early on how much a patient will benefit from DIBH.
248 This research sought to reveal the impact of abdominal breath-holding on
249 knowledge-based treatment planning for breast cancer radiotherapy so that we can
250 guide the application of DIBH more precise before treatment.

251 In this study, two KDE-based dose prediction models with two different
252 respiratory patterns of FB and DIBH for IMRT treatment were established. The
253 contrast of both FB and DIBH IMRT plans in the original 40 patients, created by
254 manual and KBP method, shows that KBP plans provided at least comparable plan
255 quality compared to clinical ones ($p > 0.05$).

256 The further comparative study was performed in another 10 patients similar to
257 the training datasets. There was no significant difference between $Plan_{FB-CT}^{FB\ mod\ el}$ and
258 $Plan_{FB-CT}^{manual}$ or $Plan_{DIBH-CT}^{DIBH\ mod\ el}$ and $Plan_{DIBH-CT}^{manual}$. The acceptable P-values indicate that
259 our model provides good estimates for DVHs in the same breath settings. A counsel
260 of perfection of $Prediction_{FB-CT}^{DIBH\ mod\ el}$ makes unachievable objective targets for
261 $Plan_{FB-CT}^{DIBH\ mod\ el}$. The average OAR dose for $Prediction_{DIBH-CT}^{FB\ mod\ el}$ was higher than
262 $Plan_{DIBH-CT}^{manual}$ ($p < 0.05$ for all clinically relevant structures), and the estimated mean
263 dose was slightly higher than the delivered one. It could be due to part of FB model
264 predicted constraint conditions were too relaxed to limit the dose of OARs.

265 Figure 2 shows one representative example of four situations of the DVHs cross-
266 validated by two KDE models. The dashed line represents the deliverable plan and the
267 solid line represents the KDE prediction. The DVHs of the heart, LADCA, and

268 left-lung were shown in the black lines, red lines, and green lines, respectively.



269

270 **Figure 2:** The DVHs of the prediction (solid line) and the deliverable plan
271 (dashed line) for (a)FB model work with FB-CT; (b)DIBH model work with FB-CT;
272 (c) FB model work with DIBH-CT; (d) DIBH model work with DIBH-CT.

273

274 All in all, in order to more easily and accurately guide the application of deep
275 inhalation and breath-holding in left breast cancer radiotherapy, we must quantify the
276 protective capacity of DIBH for normal organs. As a method of evaluation, the KBP
277 improves the consistency of all IMRT plans by minimizing the dissimilarity in plan
278 quality due to the variation planner. To create the scoring flow that classifies new
279 patients do the following: put FB-CT and DIBH-CT scans of the left-breast patient
280 into correspondence KDE model, then we can distinguish who would benefit from
281 DIBH more by comparison and analysis.

282 Evidently selecting the appropriate KBM model in this link is crucial. This

283 present work has demonstrated that one KDE model trained with one breath condition
284 may not suitable for all breath conditions. FB model cannot predict DIBH-CT
285 precisely because the establishment of FB model constraints is too loose for
286 DIBH-CT. This may cause plan quality degradation. Meanwhile, there are two
287 problems when using the DIBH model work with FB-CT: one is difficult for plan
288 generation due to the harsh prediction constraints; the other is overtime for plan
289 optimization. However, it is necessary to examine the effect of enlarging the sample
290 size on the model presented in future research.

291

292 **Conclusions**

293 The current work developed a KBP model for functional-guided radiotherapy.
294 Modest, but statistically significant, improvements were observed in LAD, functional
295 lung and heart doses of individual model corresponding to CT breathing patterns.
296 Thus, in order to obtain superior performance in a knowledge-based treatment
297 planning, different breathing conditions should be taken into account.

298 We consider this study innovative because it explains and validates the
299 correlation between classification of the KDE based dose prediction model and
300 breathing maneuvers during left-sided whole-breast irradiation after breast-conserving
301 surgery. It shows that classifying KDE dose prediction models according to
302 respiratory patterns are indispensable, thus an optimal decision base for automatically
303 making the radiation therapy plan of the marshalling station with computer is supplied.
304 This research, while just a beginning, at least establishes some basic scientific facts

305 that could prove useful in future studies on the automatic plan and related conditions.

306

307 **Declarations**

308 **Ethics approval and consent to participate**

309 This prospective study was conducted in compliance with the ethical principles of the
310 Declaration of Helsinki and was approved by the Research Ethics Committee of the
311 First Affiliated Hospital, College of Medicine, Zhejiang University. Informed consent
312 was obtained from all individual participants included in the study.

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319 **Availability of data and materials**

320 The datasets used and/or analysed during the current study are available from the
321 corresponding author on reasonable request.

322 **Consent for publication**

323 Not applicable

324 **Competing interests**

325 The authors declare that they have no competing interests

326 **Authors' contributions**

327 JQX: literature search, figures, study design, data analysis, tables, figures,
328 interpretation, manuscript writing and paper revision; JZW, WGH: study design, data
329 collection, manuscript writing and paper revision; FZ, GRY, LYB: study design,
330 radiotherapy planning, data collection, data analysis, interpretation and paper revision;
331 ZJL,SXY: study design, data analysis, interpretation, figures and paper revision; All
332 authors have read and approved the final version of the manuscript.

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335

336

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403 **Figure legends:**

404 Figure 1: The strategy of knowledge-based planning generated optimization
405 objectives

406 Figure 2: The DVHs of the prediction (solid line) and the deliverable plan (dashed
407 line) for (a)FB model work with FB-CT; (b)DIBH model work with FB-CT; (c)DIBH
408 model work with DIBH-CT; (d)FB model work with DIBH-CT.

Figures

<u>THE WORKFLOW OF THIS STUDY</u>		<u>PERFORMANCE EVALUATION</u>	
<div style="text-align: center;"> Two CT scans (FB and DIBH) ↓ Model training (FB and DIBH) ↓ Model cross prediction ↓ Performance evaluation </div>	FB-CT	FB model	DIBH model
		Clinical plan VS. KDE prediction	Clinical plan VS. KDE prediction
	DIBH-CT	KDE plan VS. KDE prediction	KDE plan VS. KDE prediction
		Clinical plan VS. KDE prediction	Clinical plan VS. KDE prediction
		KDE plan VS. KDE prediction	KDE plan VS. KDE prediction

Figure 1

The strategy of knowledge-based planning generated optimization objectives

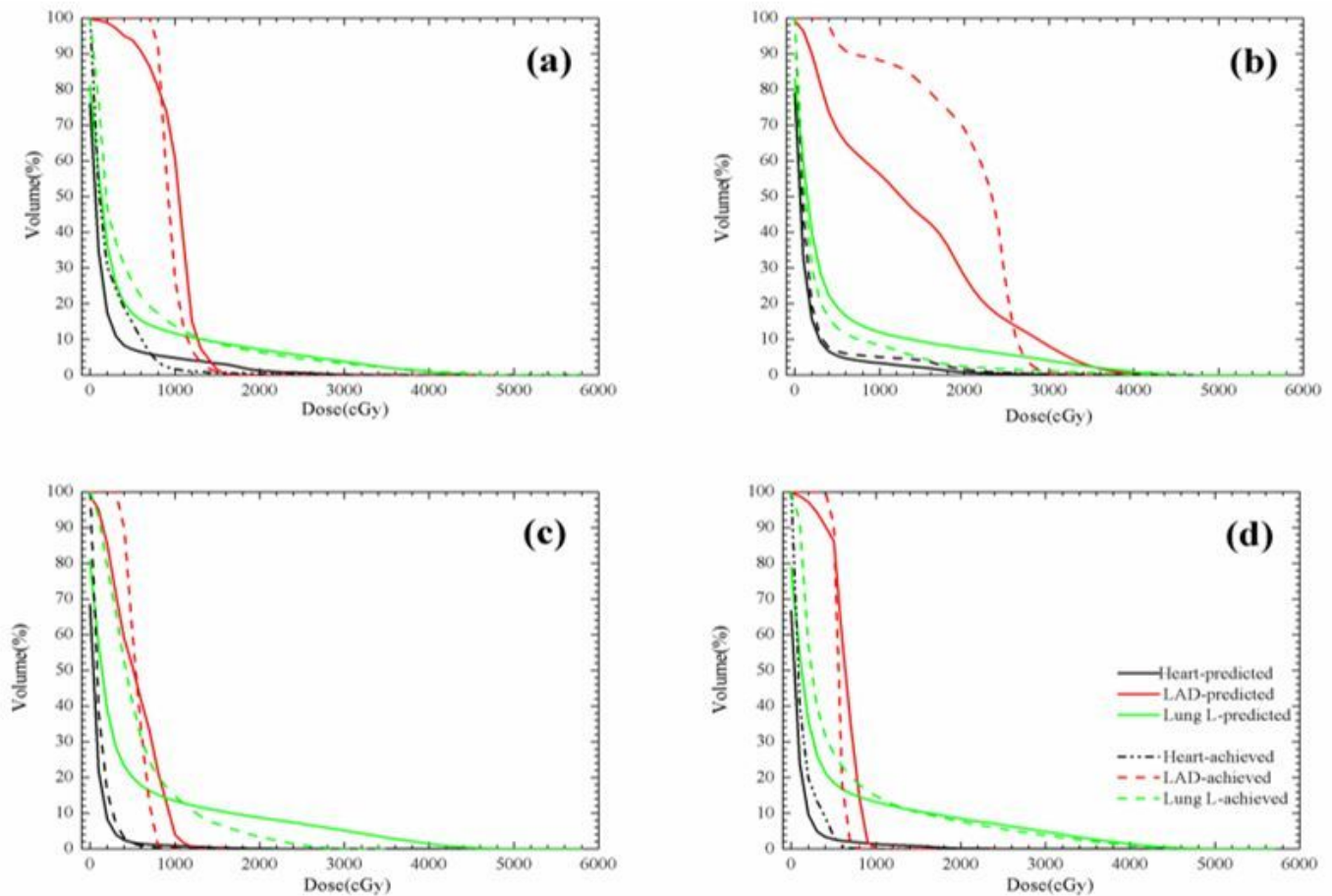


Figure 2

The DVHs of the prediction (solid line) and the deliverable plan (dashed line) for (a)FB model work with FB-CT; (b)DIBH model work with FB-CT; (c) FB model work with DIBH-CT; (d) DIBH model work with DIBH-CT.